

PATENT

IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

In re Application of:  
Dhiraj SARDAR *et al.*

Serial No.: 10/543,001

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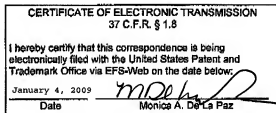
For: METHOD AND APPARATUS FOR  
DIAGNOSING NEOVASCULARIZED  
TISSUES

Group Art Unit: 3768

Examiner: Joel F. BRUTUS

Atty. Dkt. No.: UTSJ:041US

Confirmation No.: 1190



**DECLARATION OF ANDREW TSIN UNDER 37 C.F.R. §1.132**

I, Andrew Tsin, hereby declare as follows:

1. I am a citizen of the United States residing at 8125 Triple Crown, Fair Oaks Ranch, Texas, 78015, USA.
2. I am a Professor of Biochemistry and Cell Biology in the Department of Biology at the University of Texas at San Antonio and an Adjunct Professor of Ophthalmology in the Department of Ophthalmology at the University of Texas Health Science Center in San Antonio. I have expertise in the area of ocular biochemistry and cell biology, as well as ophthalmic imaging, as evidenced by my extensive publications in scientific and biophotonics journals in the areas of retinoid metabolism, angiogenic cytokines (for diabetic retinopathy and macular degeneration) and optical properties of healthy and diseased retinas. A copy of my resume is attached as Appendix A.
3. I am one of the inventors of the above-referenced patent application.

4. I have reviewed the Office Action that was mailed on August 4, 2009. I understand that the patent examiner considers the claimed invention to not be patentable because the claimed invention would be obvious to a person of ordinary skill in the field of the invention based on the teachings of the Dreher patent (U.S. Patent 5,303,709) in view of the Hay patent (U.S. Patent 5,632,282), and further in view of the Glaser patent (U.S. Patent 5,767,079), the Larrick patent (U.S. Patent 5,670,151), and/or the Trachtman patent (U.S. Patent 5,002,384). The main reference which the examiner appears to rely on is the Dreher patent.
5. The pending claims concerns methods and apparatuses for diagnosing an ocular disease involving neovascularization. The methods and apparatuses of the invention concern illumination of ocular tissue in a sample holder with a light beam and measurement of particular physical properties of light that is backscattered from the ocular tissue in the sample holder. The physical properties of the backscattered light that are measured include, for example, maximum intensity and/or a polarization shift.
6. The references cited by the patent examiner are distinct from the presently claimed invention because the references do not concern methods or apparatuses that involve measurement of a physical property of backscattered light. The Dreher patent specifically concerns methods and devices for measuring the topography and thickness of the nerve fiber layer that involve measuring the polarization shift of a *reflected* probing light. See abstract, FIG. 1, and col. 2, lines 60-68. Thus, rather than measurement of properties of backscattered light, the Dreher patent is *distinct* because it concerns measurement of a physical property of reflected light. The Trachtman patent concerns analysis of infrared light *reflected* from the patient's cornea and retina for monitoring and training eye position. The Hayes patent concerns methods for diagnosing eye disease that

involve measurement of light *reflected* from a patient's retina. The Larrick patent does not concern ophthalmic imaging, but instead concerns methods of controlling hyperproliferative disease of the integument and the eye. The Glaser patent does not concern optical diagnosis, but instead concerns an ophthalmic treatment method employing Transforming Growth Factor  $\beta$ .

7. There are fundamental differences between reflected light and backscattered light. The fundamental differences between these two types of light and matter interactions can be characterized by where the interaction of light and matter occurs, known physical laws which govern the interaction, and the types of interactions between light and matter that occur during these processes. In the most basic physical treatment, reflection is defined as the return of incident electromagnetic radiation (*i.e.*, light) by a surface. This is discussed on page 177 of Optics Source Book, Ed. Parker, Sybil P, 1988 McGraw-Hill, ISBN 0-07-045506-6 (Exhibit A) and page 79 of Optics, Hecht E, 1987 Addison-Wesley Publishing, ISBN 0-201-11609-X (Exhibit B). For an incident beam of light, there exists a number of fundamental laws which describe how the direction of the light is changed by interaction with a "reflective" surface. The law of reflection states that the angle of incidence of light is directly equal to that of the reflected light (see Exhibit A and page 83 of Optics cited above (Exhibit C)). Reflectivity, or a direct measure of the amount of radiation reflected by a material, is dependent upon the angle of incidence, polarization state of incoming radiation, and the electromagnetic properties of the material.
8. In the case of scattered light, of which backscattered light is merely a special case where the angle of scattering is greater than 90 degrees, the interaction between light and matter is approached from a microscopic point of view. Scattering is described as the removal of energy from an incident wave and the subsequent remission of some portion of that

energy. This is discussed on page 293 of Optics cited above (Exhibit D). The angle at which the scattered photon is remitted is highly dependent upon the type of scattering which it undergoes. In complex structures, such as tissue, there are often multiple scattering events from the time the photon enters the material to the time it exits the material. Thus, a photon which is scattered only once will have a different final direction than a photon which is scattered three or four times. This is ultimately responsible for the statistical nature of scattered light in tissues. Due to the optically non-homogenous properties of biological tissues, it is not uncommon to see reflection at the surface, as well as transmission and scattering through biomaterials (see page 3 of Tissue Optics, Tuchin V, 2000 SPIE Press, ISBN: 0-8194-3459-0 (Exhibit E)).

9. In the specific case of the present invention, backscattered light is light that is scattered in such a way that it finds its way back towards the light source and occurs at a range of depths into the tissue.
10. In the Dreher patent, it is specifically stated that the light reflected off of the posterior or anterior surfaces of the eye offers the method of detection (see Column 2 Line 64, Column 3 Line 9, Column 5 Line 1, Column 5 Line 47, Column 10 Line 14). In contrast, the present invention utilizes light which is backscattered throughout the entirety of a tissue layer. More so, it is clearly stated in the Dreher patent that the aim of the device is to determine optic nerve thickness by exploitation of the birefringence properties of that tissue (Column 3 Line 65 – Column 4 Line 20), whereas the present claimed invention seeks to determine degree of a pathological condition (neovascularization as exemplified by angiogenesis of retinal or choroidal capillaries). Thus, there are distinct differences between the methods and apparatuses of the Dreher patent and the present invention.

11. Further, the apparatuses described in the Dreher patent require use of a "corneal polarization compensator." See abstract. The present invention does not involve use of a corneal polarization compensator. Use of this additional component in the context of the present invention would result in loss of information in that it would likely result in loss of some portion of backscattered light. Therefore, one of ordinary skill the field would not be likely to successfully practice the claimed methods of diagnosing an ocular disease involving neovascularization with the apparatuses of the Dreher patent.
12. Given the fundamental differences between the light that is being measured in the Dreher patent (and other cited patents) and the present invention and the requirement for a corneal polarization compensator in the Dreher patent, a person with training in ophthalmic imaging and optics would not have been motivated to modify the Dreher patent or combine it with any of the other references cited by the Examiner to result in the claimed methods and apparatuses. None of the references cited by the patent examiner concern analysis of backscattered light, which is the heart of the present invention.
13. I hereby declare that all statements made herein of my knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under Section 1001 of Title 18 of the United States Code and that such willful false statements may jeopardize the validity of the application or any patent issued thereon.

Date

January 4, 2010

Andrew Tsin, Ph.D.

Professor

## BIOGRAPHICAL SKETCH

Provide the following information for the key personnel and other significant contributors in the order listed on Form Page 2.  
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Dalhousie University, Halifax, N.S., Canada	BSc	1973	Biology
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University of Alberta, Edmonton, AB, Canada	Ph.D.	1979	Zoology
Baylor College of Medicine, Houston, Tx, USA	Pdf	1979-81	Ophthalmology

### A. Positions and Honors:

#### APPOINTMENTS:

- 1990-Present Professor, Dept. of Biology, University of Texas at San Antonio (UTSA)
- 1990-Present Adjunct Professor, Department of Ophthalmology, U of Texas HSC-SA
- 1991-Present Director, MBRS-SCORE Program, UTSA
- 2007-Present Director, Center for Research and Training in the Sciences, UTSA
- 2008-Present Director, Research Center in Minority Institutions, UTSA
- 2008-Present Associate Dean of Research, College of Sciences, UTSA

#### FEDERAL GOVERNMENT ADVISORY COMMITTEE:

- NSF Reviewer and Panelist, (1987-present)
- NIH Reviewer and Site visit Team, (1987-present)
- HRSA Reviewer, (1986-1999)
- NIH-NIGMS Review Subcommittee, (1999-2003)

### B. Selected Peer-Reviewed Publications: (Publications #1-23 published between 1977-1986)

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### **C. Research Support:**

#### **Ongoing Research Support**

- |   |             |                   |
|---|-------------|-------------------|
| FY10/11   | Sardar (PI) | 9/01/09-8/31/10   |
| Collaborative Research Seed Grant Program   |             |                   |
| Development of Novel Biomedical Probes Incorporating Rare-Earth Nanocrystals.   |             |                   |
| The development of novel targeted contrast agents from nanomaterials for medical imaging by a multidisciplinary approach which includes physics, biology and chemistry. |             |                   |
| Role: Co-Investigator   |             |                   |
| 5G12RR013646-10   | Romo (PI)   | 08/01/08-07/31/10 |
| NIH/NCRR/RCMI   |             |                   |
| Cajal Neuroscience Research Center (CNRC)   |             |                   |
| Establishment of neuroscience research to support core facilities and faculty research at UTSA.   |             |                   |
| Role: Program Director  |             |                   |
| 5K03  | Tsin (PI)   | 12/06/07-2/28/10  |
| Kronosky Foundation   |             |                   |
| A Study in Diabetic Eye Disease – Damage in Diabetic Retinopathy Due to Acrolein and its Mitigation by NBHA.  |             |                   |
| A study on the effect of acrolein on the levels of oxidized proteins and cytokines in eye and its mitigation by NBHA.   |             |                   |
| Role: PI  |             |                   |

#### **Completed Research Support**

- |  |           |                    |
|--|-----------|--------------------|
| POC-RR 1300  | Tsin (PI) | 12/01/08 – 8/31/09 |
| South Texas Technology Management – Texas Emerging Technology Fund/Office of the Governor of Texas                               |           |                    |
| Adaptive Optics and Retinal Imaging  |           |                    |
| The goal of this study was to construct a prototype of an adaptive optical system as a diagnostic instrument for retinal imaging |           |                    |
| Role: PI   |           |                    |
| GM 08194-26  | Tsin (PI) | 8/01/04 -7/31/07   |
| NIH/NIGMS  |           |                    |
| Pathway of the Cone Visual Cycle   |           |                    |
| The goal of this project was to study the biochemical pathway of the novel cone visual cycle in the vertebrate retina.           |           |                    |
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Cover: infrared thermogram showing thermal effluent entering a glow-discharge stream with flow from left to right. (Barnes Engineering Co.)

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## TABLE OF CONTENTS

Introduction	1
Geometrical Optics	3
Optical Imaging Systems	39
Physical Nature of Light	107
Wave Optics	131
Interaction of Light with Matter	175
Interaction of Light with Energy	
Fields	245
Lasers: Technology and Applications	261
Light Detection and Processing	307
Measurement of Light	341
Human Perception of Light	385
Contributors	385
Index	391





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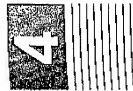
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that  $\lambda_0 \rho_0 = c$ . This formulation is a consideration of the Cauchy equation, that where  $\lambda \gg \lambda_0$ . Cauchy's equation is an extension of Sellmeier's. First, write the above with only the first term in the sum; expand the binomial theorem; take the square root of  $n$  and again.

If an ultraviolet photon is to dissociate the oxidized carbon atoms in the carbon monoxide, it must provide 11 eV of energy. What is the frequency of the appropriate radiation?



# THE PROPAGATION OF LIGHT

## 4.1 INTRODUCTION

We now consider a number of phenomena related to the propagation of light and its interaction with material media. In particular, we shall study the characteristics of light waves as they progress through various substances, crossing interfaces, and being reflected and refracted in the process. For the most part, we shall envision light as a classical electromagnetic wave whose velocity through any medium is dependent upon that material's electric and magnetic properties. It is an intriguing fact that many of the basic principles of optics are predicated on the wave aspects of light but are completely independent of the exact nature of the wave. As we shall see, this accounts for the longevity of *Huygens's principle*, which has served in turn to describe mechanical ether waves, electromagnetic waves, and now, after three hundred years, applies to quantum optics.

Suppose, for the moment, that a wave impinges on the interface separating two different media (e.g., a piece of glass in air). As we know from our everyday experiences, a portion of the incident flux density will be diverted back in the form of a *reflected wave*, while the remainder will be transmitted across the boundary as a *refracted wave*. On a submicroscopic scale we can envision an assemblage of atoms that scatter the incident radiant energy. The manner in which these emitted light waves superimpose and combine with each other will depend on the spatial distribution of the scattering

atoms. As we know from the previous chapter, the scattering process is responsible for the index of refraction, as well as the resultant *reflected* and *refracted* waves. This atomistic description is quite satisfying conceptually, even though it is not a simple matter to treat analytically. It should, however, be kept in mind even when applying macroscopic techniques, as indeed we shall later on.

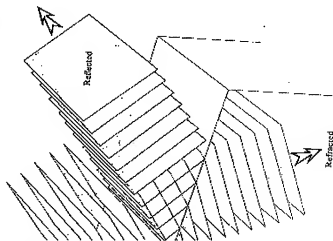
We now seek to determine the general principles governing or at least describing the propagation, reflection, and refraction of light. In principle it should be possible to trace the progress of radiant energy through any system by applying Maxwell's equations and the associated boundary conditions. In practice, however, this is often an impractical if not an impossible task (see Section 10.1). So we shall take a somewhat different route, stopping, when appropriate, to verify that our results are in accord with electromagnetic theory.

## 4.2 THE LAWS OF REFLECTION AND REFRACTION

### 4.2.1 Huygens's Principle

Recall that a wavefront is a surface over which an optical disturbance has a constant phase. As an illustration, Fig. 4.1 shows a small portion of a spherical wavefront  $S$  in a homogeneous medium. Clearly, if the radius of the wavefront as shown is  $r$ , at some later time  $t$  it will simply be  $(r + vt)$ , where  $v$  is the phase velocity of the wave.

suppose the incident wave comes in at some angle, as indicated in Fig. 4.5. Clearly, it sweeps the interface again, essentially splitting into two: one reflected and one refracted. Let's follow the path of a typical front in Fig. 4.6, envisioning the interface as if it were a series of snapshots taken in intervals of time  $\tau$ . Start when  $\Sigma_1$  makes it to the interface at point  $a$ . At that point, both the incident and transmitted wavefronts begin, so  $a$  is on both fronts, can be taken as a source of upwardly emitted wavelet traveling at a speed  $v_1$  in the incident medium and at a speed  $v_2$  in the second medium. Now focus on another point, say,  $b$  on  $\Sigma_1$ . At time  $t_1$  the plane  $\Sigma_1$  will have moved a distance  $b'f$ . Presumably, two wavelets will then propagate from  $b'$  into the incident and transmitting media, contributing to the reflected,  $\Sigma_r'$ , and transmitted wavefronts. These wavelets are shown here after where  $\tau = t_1 + t_2$ . The rest of the diagram



Reflected and transmitted wavefronts at a given instant.

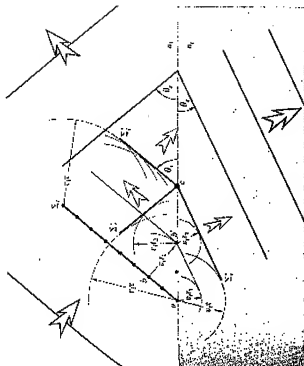


Figure 4.6 Reflection and transmission at an interface via Huygens's principle.

should be self-explanatory. Figure 4.7 is a somewhat simplified version in which  $\theta_i$ ,  $\theta_r$ , and  $\theta_t$ , as before, are the angles of incidence, reflection, and transmission (or refraction), respectively. Notice that

$$\frac{\sin \theta_i}{BD} = \frac{\sin \theta_r}{AC} = \frac{\sin \theta_t}{AE} = \frac{1}{\lambda D} \quad (4.1)$$

By comparison with Fig. 4.6, it should be evident that

$$BD = v_1 t, \quad AC = v_1 t, \quad AE = v_2 t, \quad (4.2)$$

so substituting into Eq. (4.1) and canceling  $t$ , we have

$$\frac{\sin \theta_i}{v_1} = \frac{\sin \theta_r}{v_1} = \frac{\sin \theta_t}{v_2}. \quad (4.3)$$

It follows from the first two terms that the angle of incidence equals the angle of reflection, that is,

$$\theta_i = \theta_r.$$

Known as the law of reflection, it first appeared in the book entitled *Catoptrics*, which was purported to have been written by Euclid.

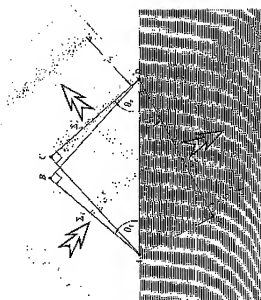


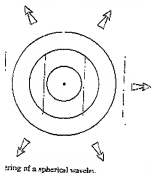
Figure 4.7 Reflected and transmitted wavefronts at a given instant.



## SCATTERING AND POLARIZATION

### Introduction to Scattering

In order to understand many apparently unrelated atomic processes, and so we again return to it. When an electromagnetic wave impinges on an atom or molecule it interacts with the bound electron, imparting energy to the atom. The effect is as if the lowest energy or ground state of the atom were set into vibration. The oscillatory motion of the electron cloud is equal to the driving force, that is, the frequency of the harmonic lightwave. The amplitude of the oscillation is relatively large only when  $\nu$  is in the vicinity of the natural frequency of the atom. In fact, at resonance we employ the simple description of the atom as a harmonic oscillator; upon absorbing a photon (an effect known as *resonance radiation*), it makes the transition to an excited state. In dense media, the atoms do not return to their ground state, having dissipated energy thermally. In rarefied gases the atoms usually make the downward transition by emitting a photon. In this process, the electron with respect to the nucleus may be regarded as an electric dipole, and as such they will



Scattering of a spherical particle.

generally reradiate electromagnetic energy at a frequency coinciding with that of the incident light. This reradiation propagates out in the dipole radiation pattern of Fig. 8.31. The removal of energy from an incident wave and the subsequent reradiation of some portion of that energy is known as *scattering* (Fig. 8.33). It is the underlying physical mechanism operative in reflection, refraction, and diffraction; the scattering process is fundamental indeed.

In addition to electron-oscillators, which generally have resonances in the ultraviolet, there are atomic-oscillators, which correspond to the vibration of the constituent atoms within a molecule. Because of their large masses, atomic-oscillators usually have resonances in the infrared. Moreover, they have relatively small vibrational amplitudes and are therefore of little concern here.

The amplitude of an oscillator, and thus the amount of energy removed from the incident wave, increases as the frequency of the wave approaches a natural frequency of the atom. For low-density gases, in which atomic interactions are negligible, absorption will be insignificant, and the reradiated or scattered wave will carry off increasingly more energy as the driving frequency approaches a resonance. This results in some rather interesting effects when the atom's natural frequencies are in the ultraviolet and the incident wave is in the visible region. In that case, as the frequency of the incoming light increases, more and more of it will be elastically scattered. As an example, imagine that you are outside on a bright clear morning. The sky is a brilliant blue, and you are surrounded, even inundated, with blue light. Sunlight streaming into the atmosphere from one direction is scattered in all directions by the air molecules. Without an atmosphere, the daytime sky would be as black as the void of space, a point well made in the Apollo lunar photographs (Fig. 8.34). You would then see only light that shone directly at you. With an atmosphere, the red end of the spectrum is, for the most part, unscattered, whereas the blue or high-frequency end is substantially scattered. This high-frequency scattered light reaches the observer from many directions, making the entire sky appear bright and blue (Fig. 8.35). When the Sun is very low in the sky, its rays pass through a great thickness of air. The

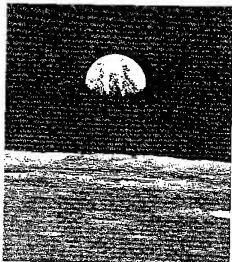


Figure 8.34 A half-Earth hanging in the black Moon sky. (Photo courtesy NASA)

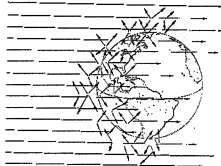


Figure 8.35 Scattering of sky light.

# TISSUE OPTICS

## Light Scattering Methods and Instruments for Medical Diagnosis

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To my grandkids,  
Dasha, Zhenya, and Stepa

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# OPTICAL PROPERTIES OF TISSUES WITH STRONG (MULTIPLE) SCATTERING

This first chapter introduces the problem of light (laser beams) transport within strongly (multiple) scattering tissues, such as skin, breast, brain, and vessel wall. Basic principles and theoretical descriptions using radiation transfer theory or Monte Carlo (MC) simulation are considered. Methods for solving the inverse problem of finding tissue optical parameters and their advantages and drawbacks are analyzed. Since contrast of optical images always depends on the optical properties of the tissues under investigation, the specifics of controlling tissue optical parameters are considered. The propagation of short pulses and photon-density diffusion waves in scattering and absorbing media is analyzed and the prospects of these methods for tissue spectroscopy and tomography are discussed. Polarization phenomena and optothermal and optoacoustic interactions in strongly scattering tissues are described. A discrete-particle model of soft tissue is presented. The design and characterization of tissue-like phantoms for optical diagnostics are described.

## 1.1 PROPAGATION OF CONTINUOUS WAVE LIGHT IN TISSUES

### 1.1.1 Basic principles and major absorbers

Biological tissues are optically inhomogeneous and absorbing media whose average refractive index is higher than that of air. This is responsible for partial reflection of the radiation at the tissue/air interface (Fresnel reflection), while the remaining part penetrates the tissue. Multiple scattering and absorption are responsible for laser beam broadening and eventual decay as it travels through a tissue, whereas bulk scattering is a major cause of the dispersion of a large fraction of radiation in the backward direction. Cellular organelles such as mitochondria are the main scatterers in various tissues.

Absorbed light is converted to heat or radiated in the form of fluorescence, it is also consumed in photochemical reactions. The absorption spectrum depends on the type of predominant absorption centers and water content of tissues (see Figures 1.1-1.4). Absolute values of absorption coefficients for typical tissues lie in the range  $10^{-2}$  to  $10^4 \text{ cm}^{-1}$ , 1-4, 6, 9-15, 28, 29, 31, 37-42, 56, 57, 72, 86-91. In the ultraviolet (UV) and infrared (IR) ( $\lambda \geq 2 \mu\text{m}$ ) spectral regions, light is readily absorbed,